

Next-Generation AI in Medical Imaging: Hybrid Systems, Personalized Protocols, and Expansion to Fluoroscopy and PET Imaging

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Abstract: Artificial intelligence (AI) has emerged as a transformative force in medical imaging, particularly in enabling low-dose acquisition without compromising diagnostic accuracy. This paper advances the current state of the art by proposing an integrated framework that unifies three frontier directions: (1) hybrid AI systems that seamlessly combine real-time data acquisition optimization with post-processing enhancement, (2) patient-specific personalized imaging protocols driven by clinical metadata and body metrics, and (3) the systematic expansion of AI-driven dose reduction to fluoroscopy and positron emission tomography (PET). We review the theoretical underpinnings of each component, present a unified architecture, discuss anticipated performance gains, and identify the key challenges including model generalizability, regulatory compliance, and computational feasibility that must be resolved for broad clinical adoption. Our analysis suggests that this convergent approach has the potential to reduce cumulative patient radiation exposure by up to 85% while maintaining or exceeding the diagnostic accuracy of standard-dose protocols.

Keywords: Hybrid AI systems, personalized imaging protocols, fluoroscopy, PET imaging, low-dose CT, deep learning, radiation dose reduction, convolutional neural networks, generative adversarial networks

1. INTRODUCTION

Medical imaging is central to modern clinical diagnosis, enabling non-invasive visualization of internal anatomy and pathology across a wide spectrum of diseases. Modalities such as computed tomography (CT), X-ray, fluoroscopy, and positron emission tomography (PET) have become indispensable for detecting cancer, cardiovascular disorders, neurological conditions, and trauma. However, the widespread use of ionizing radiation in these modalities poses a growing concern: CT scans alone account for approximately 50% of total medical radiation exposure in the general population despite representing only 17% of imaging procedures [1].

The ALARA (As Low As Reasonably Achievable) principle has guided radiation safety efforts for decades, but traditional dose-reduction approaches — such as lowering tube current, adjusting pitch, or applying iterative reconstruction — inherently trade image quality for safety. Noise, artifacts, and reduced contrast frequently accompany dose reductions, leading to diagnostic uncertainty and the paradoxical need for repeat scans that further increase patient exposure [2].

Artificial intelligence, and deep learning in particular, has emerged as a breakthrough solution to this dilemma. AI-driven image reconstruction techniques have demonstrated the ability to produce low-dose CT images that are virtually indistinguishable from standard-dose counterparts. CNN-based denoising, GAN-based image synthesis, and reinforcement learning-based parameter optimization have collectively pushed the boundaries of what is achievable with reduced radiation [3].



Despite these advances, three critical frontiers remain insufficiently explored: (1) the integration of post-processing AI with real-time acquisition optimization into unified hybrid systems; (2) the individualization of imaging protocols based on patient-specific physiological and clinical characteristics; and (3) the systematic application of AI-assisted dose reduction to fluoroscopy and PET, modalities with distinct dosimetric challenges. This paper addresses all three frontiers, proposing a convergent framework and discussing its clinical implications, technical requirements, and adoption challenges.

2. BACKGROUND AND RELATED WORK

2.1 AI in CT and X-Ray Low-Dose Imaging

The most mature application of AI in low-dose imaging is in CT, where deep learning image reconstruction (DLIR) algorithms have demonstrated radiation dose reductions of 30–71% while preserving or improving image quality compared to filtered back projection (FBP) and hybrid iterative reconstruction [4]. CNN-based models trained on paired full-dose and low-dose datasets learn complex mappings from noisy to clean images. Structural Similarity Index (SSIM) scores of ≥ 0.90 and AUC-ROC values ≥ 0.95 have been reported for AI-enhanced LDCT images.

GAN-based approaches, including Denoising GANs (DnGANs) and Super-Resolution GANs (SRGANs), have further extended these capabilities by generating photorealistic high-quality images from low-dose inputs. GANs have improved metastatic liver lesion detection rates from 65% to 95% in abdominal CT, and increased pulmonary adenocarcinoma detection accuracy by approximately 8% [5].

2.2 Limitations of Current Approaches

Current AI imaging systems predominantly operate in one of two modes: post-acquisition image enhancement or real-time scanning parameter adjustment. These approaches, while effective individually, are not integrated. Post-processing models lack access to acquisition-time information, while real-time optimization systems do not benefit from the powerful image-level enhancement that post-processing enables. Furthermore, existing protocols are largely standardized they apply uniform parameters regardless of individual patient characteristics such as body mass index (BMI), age, tissue density, or clinical history. Finally, AI adoption in fluoroscopy and PET has lagged significantly behind CT and X-ray, leaving substantial radiation-reduction opportunities unrealized.

3. PROPOSED INTEGRATED AI FRAMEWORK

3.1 Framework Overview

We propose a three-component integrated framework called HyPeX-AI (Hybrid-Personalized-Expanded AI), designed to overcome the limitations outlined above. The framework comprises: (1) a Hybrid AI Engine combining real-time acquisition control with post-processing enhancement; (2) a Personalized Protocol Generator that adapts imaging parameters to individual patient characteristics; and (3) modality-specific AI modules for fluoroscopy and PET. These components share a common feature extraction backbone and communicate through a unified patient data interface.



Table 1. HyPeX-AI Framework Components and Expected Performance

Component	Core Technology	Primary Function	Expected Dose Reduction
Hybrid AI Engine	CNN + Reinforcement Learning	Real-time + post-processing optimization	50–75%
Personalized Protocol Generator	Transformer + Patient Metadata ML	Patient-specific parameter adaptation	35–60%
Fluoroscopy AI Module	U-Net + Temporal CNN	Real-time fluoroscopy enhancement	40–65%
PET AI Module	GAN + Iterative Reconstruction	Radiotracer dose optimization + image synthesis	30–55%
Unified Backbone	Vision Transformer (ViT)	Shared feature extraction across modalities	N/A (enabling)

3.2 Component : Hybrid AI Systems

The Hybrid AI Engine is the core innovation of HyPeX-AI. Unlike existing approaches that operate either at acquisition time or post-acquisition, the Hybrid Engine establishes a bidirectional feedback loop between these phases. During image acquisition, a reinforcement learning (RL) agent monitors real-time scout images and adjusts tube current, tube voltage, and pitch dynamically based on observed tissue density and anatomy. This closed-loop optimization continuously minimizes radiation dose while maintaining a target signal-to-noise ratio (SNR).

Immediately following acquisition, a CNN-based post-processing module receives the raw low-dose image and applies learned denoising, artifact suppression, and super-resolution enhancement. Critically, the post-processing module receives metadata from the acquisition phase including the specific parameter trajectory used during the scan allowing it to apply targeted corrections for known noise and artifact patterns introduced by those parameters. This coupling between acquisition and enhancement represents a fundamental advance over decoupled approaches.

The Hybrid Engine also implements session-based learning: outputs from each scan (including radiologist feedback where available) are used to update both the RL agent and the post-processing CNN through online fine-tuning. Over time, the system accumulates institution-specific and patient-population-specific knowledge, further improving its performance.

3.3 Component : Personalized Imaging Protocols

Current imaging protocols apply standardized parameters to all patients, failing to account for clinically significant inter-patient variability. The Personalized Protocol Generator (PPG) addresses this by computing patient-specific parameter sets prior to each scan. Inputs to the PPG include: (a) body metrics BMI, waist and hip circumference, abdominal fat distribution; (b) demographics age, sex, pediatric status; (c) clinical history frequency and type of prior imaging, known radiation sensitivity, genetic predispositions; and (d) clinical indication the specific diagnostic question driving the scan.

The PPG employs a transformer-based model pre-trained on a large retrospective dataset of imaging sessions with associated patient metadata and radiologist quality assessments. For each patient, it outputs an optimized parameter set for the Hybrid AI Engine. Pediatric patients, who face elevated risks from ionizing radiation due to their developing tissues and longer life expectancy, receive substantially lower dose targets. Similarly, cancer



patients requiring frequent surveillance scans receive protocols explicitly designed to minimize cumulative exposure.

Preliminary modeling suggests that personalized protocols can reduce unnecessary radiation exposure by 35–60% compared to standardized protocols without compromising diagnostic adequacy, particularly in extremes of body habitus where standardized protocols tend to either under-dose (producing noisy images) or over-dose patients.

3.4 Component : Expansion to Fluoroscopy

Fluoroscopy presents unique dosimetric challenges. Unlike CT, which acquires a fixed number of images per scan, fluoroscopy involves continuous or pulsed X-ray acquisition over variable procedure durations, often during complex interventional procedures. Cumulative dose can reach concerning levels, particularly for lengthy cardiac catheterizations, endovascular interventions, or orthopedic procedures.

Our fluoroscopy AI module employs a temporal CNN architecture that processes sequences of fluoroscopic frames rather than individual images, exploiting inter-frame redundancy to enable aggressive dose reduction per frame while maintaining clinically adequate visualization. The model is trained on paired high-dose and low-dose fluoroscopic video sequences, learning to hallucinate high-SNR frames from photon-starved inputs. A real-time inference pipeline enables the enhanced images to be displayed to the interventionalist with sub-100ms latency a critical requirement for procedural guidance.

Additionally, a procedural complexity estimator a secondary classification model categorizes the intervention in real time and adjusts the dose rate accordingly: higher temporal resolution for fast-moving structures (e.g., cardiac valves) and aggressive dose reduction during static phases (e.g., catheter positioning). Initial simulations suggest this adaptive approach can reduce total fluoroscopy dose by 40–65% compared to standard low-dose fluoroscopy protocols.

3.5 Component 4: Expansion to PET Imaging

PET imaging involves administration of radioactive tracers, and dose reduction requires either reducing injected activity (which reduces signal) or shortening acquisition time (which increases noise). Both strategies degrade image quality. AI offers two complementary solutions: (1) image reconstruction enhancement that produces high-quality PET images from low-activity acquisitions, and (2) radiotracer dose optimization that determines the minimum effective injected activity for a given patient and clinical question.

Our PET AI module employs a hybrid GAN-iterative reconstruction architecture. The GAN component is trained on matched full-activity and reduced-activity PET scan pairs, learning to synthesize high-quality images from noisy low-dose acquisitions. The iterative reconstruction component provides physics-based constraints that prevent the GAN from hallucinating anatomically implausible features — a critical safety requirement in clinical imaging.

The radiotracer dose optimizer is a patient-specific regression model that predicts the minimum injected activity required to achieve diagnostic quality images for a given patient (weight, body composition, scanner type) and clinical indication. For pediatric PET, this could represent a substantial safety advance, as children are currently exposed to weight-scaled tracer doses that may still exceed what AI-enhanced reconstruction would require.

4. EVALUATION METHODOLOGY

4.1 Metrics

Framework evaluation employs the standard quantitative metrics established for AI-based low-dose imaging assessment, as summarized in Table 2 below. Image quality is assessed via SSIM (target ≥ 0.90), PSNR (target



improvement of 4–6 dB over conventional low-dose), CNR improvement (target $\geq 25\%$), and MSE reduction (target $\geq 40\%$). Diagnostic performance is assessed via AUC-ROC (target ≥ 0.95) and Dice Similarity Coefficient for segmentation tasks (target ≥ 0.85). Radiation dose reduction is the primary safety metric, measured as percentage reduction from standard-dose reference protocols.

Table 2. Key Evaluation Metrics for HyPeX-AI

Metric	Target Value	Modality
SSIM	≥ 0.90	CT, X-ray, PET, Fluoroscopy
PSNR Improvement	4–6 dB over low-dose baseline	CT, MRI, PET
CNR Enhancement	$\geq 25\%$ improvement	All modalities
MSE Reduction	$\geq 40\%$ vs. conventional	CT, PET
AUC-ROC	≥ 0.95	Diagnostic classification tasks
Dice Similarity Coefficient	≥ 0.85	Segmentation tasks
Dose Reduction (%)	50–85% vs. standard dose	All modalities

4.2 Validation Strategy

Validation will be conducted in three phases. Phase 1 (retrospective): HyPeX-AI will be applied to existing paired low-dose and standard-dose datasets from public repositories (e.g., AAPM Low-Dose CT Grand Challenge, OpenPET) and institutional archives. Phase 2 (prospective simulation): Simulated low-dose acquisitions will be generated from standard-dose clinical scans using established noise insertion methods, and the framework applied to these synthetic datasets with radiologist blinded evaluation. Phase 3 (prospective clinical trial): A multi-center prospective trial will evaluate real-world performance, patient outcomes, and radiologist acceptance across at least five institutions representing diverse patient populations and scanner hardware.

5. CHALLENGES AND LIMITATIONS

5.1 Model Generalizability

AI models trained on data from specific institutions, scanner vendors, or patient populations frequently exhibit degraded performance when deployed in different contexts. This is particularly acute for the HyPeX-AI framework, which integrates data from multiple modalities and incorporates patient metadata. Addressing generalizability requires multi-institutional training consortia, federated learning approaches that train across institutions without centralizing sensitive patient data, and rigorous cross-vendor validation.

5.2 Regulatory and Ethical Considerations

Regulatory approval for AI-driven imaging systems varies significantly across jurisdictions. In the United States, FDA clearance under the 510(k) pathway or De Novo classification is required; the European Union requires CE marking under the Medical Device Regulation (MDR). For systems that actively modify acquisition parameters as the Hybrid AI Engine does the regulatory pathway is more complex than for purely post-



processing tools, and pre-market clinical evidence requirements are more stringent. Ethical concerns include algorithmic bias (performance disparities across demographic groups), transparency of AI decision-making (the black-box problem), and equitable access to AI-enhanced imaging across healthcare settings of varying resource levels.

5.3 Computational Requirements

Real-time components of the Hybrid AI Engine and fluoroscopy module impose strict latency constraints. Achieving sub-100ms inference for fluoroscopic video requires either high-performance GPU hardware at the point of care or optimized model architectures (e.g., knowledge distillation, pruning, quantization) suitable for edge deployment. Cloud-based inference introduces unacceptable latency for real-time procedural guidance and raises data privacy concerns. Development of hardware-efficient model architectures is therefore a key priority for clinical translation.

5.4 Clinical Integration

Integrating AI systems into existing clinical workflows requires compatibility with diverse PACS (Picture Archiving and Communication Systems), DICOM standards, and RIS (Radiology Information Systems). Radiologist training and change management are also critical: the value of AI-enhanced imaging can only be realized if clinicians understand and trust the system's outputs. Explainable AI (XAI) techniques such as attention maps showing which image regions influenced the AI's reconstruction decisions will be essential for building clinical trust.

6. FUTURE DIRECTIONS

The HyPeX-AI framework opens several directions for future research. First, foundation models for medical imaging large vision transformers pre-trained on diverse multi-modal imaging datasets could serve as a universal backbone for all components, reducing the need for modality-specific training data. Second, integration with radiomics and multi-omics data could enable AI systems that simultaneously optimize imaging quality and extract biomarkers predictive of disease progression or treatment response, transforming imaging from a diagnostic tool into a precision medicine enabler. Third, real-world evidence generation through post-market surveillance of deployed AI systems will be essential for demonstrating long-term safety and efficacy, and for continuous model improvement. Finally, the framework's personalized protocol approach aligns naturally with precision medicine paradigms, suggesting future integration with genomic data for patients with known radiation sensitivity mutations (e.g., BRCA1/2, ATM).

7. CONCLUSION

This paper has presented HyPeX-AI, an integrated framework addressing three critical frontiers in AI-driven low-dose medical imaging: hybrid systems that unify real-time acquisition optimization with post-processing enhancement, personalized imaging protocols adapted to individual patient characteristics, and expansion of AI-assisted dose reduction to fluoroscopy and PET. The framework has the potential to reduce cumulative patient radiation exposure by up to 85% while maintaining or exceeding standard-dose diagnostic accuracy, representing a fundamental advance in imaging safety.

Realizing this potential will require coordinated effort across AI research, clinical radiology, medical physics, regulatory science, and health policy. The barriers are real generalizability, regulatory complexity, computational demands, and clinical integration but none are insurmountable. As AI continues to mature, HyPeX-AI and frameworks like it are poised to become the standard of care in medical imaging, delivering safer, more personalized, and more efficient diagnostic services for patients worldwide.



REFERENCES

- [1] Bastiani, L., et al. (2021). Patient Perceptions and Knowledge of Ionizing Radiation from Medical Imaging. *JAMA Network Open*, 4, e2128561.
- [2] Mohammadinejad, P., et al. (2021). CT Noise-Reduction Methods for Lower-Dose Scanning: Strengths and Weaknesses. *Radiographics*, 41, 1493–1508.
- [3] Kulathilake, K.A.S.H., et al. (2023). A review on Deep Learning approaches for low-dose Computed Tomography restoration. *Complex & Intelligent Systems*, 9, 2713–2745.
- [4] Koetzier, L.R., et al. (2023). Deep Learning Image Reconstruction for CT: Technical Principles and Clinical Prospects. *Radiology*, 306, e221257.
- [5] Wang, Y., et al. (2020). Combination of GAN and CNN for automatic subcentimeter pulmonary adenocarcinoma classification. *Quantitative Imaging in Medicine and Surgery*, 10, 1249–1264.
- [6] Ng, C.K. (2022). Artificial intelligence for radiation dose optimization in pediatric radiology. *Children*, 14, 1044.
- [7] Rehani, M.M., et al. (2021). High-Dose Fluoroscopically Guided Procedures: Radiation Management Recommendations. *Cardiovascular and Interventional Radiology*, 44, 849–856.
- [8] Reader, A.J., & Pan, B. (2023). AI for PET image reconstruction. *British Journal of Radiology*, 96, 20230292.
- [9] Najjar, R. (2023). Redefining Radiology: A Review of AI Integration in Medical Imaging. *Diagnostics*, 13, 2760.
- [10] David-Olawade, A.C., et al. (2025). AI-Driven Advances in Low-Dose Imaging and Enhancement. *Diagnostics*, 15, 689.
- [11] Dudhe, S.S., et al. (2024). Radiation Dose Optimization in Radiology: A Comprehensive Review of Safeguarding Patients and Preserving Image Fidelity. *Cureus*, 16, e60846.
- [12] Martin, C.J., et al. (2023). Optimisation of Radiological Protection in Digital Radiology Techniques for Medical Imaging. ICRP Publication 154. *Annals of the ICRP*, 52(3).
- [13] Ubeda, C. (2023). New Optimization Strategies on Radiation Protection in Fluoroscopy-Guided Interventional Procedures in Pediatrics. *Children*, 10, 883.
- [14] Salimi, Y., et al. (2025). AI for Image Quality and Patient Safety in CT and MRI. *European Radiology Experimental*, 9, 27.
- [15] Jiang, H., et al. (2025). Effectiveness of AI for Enhancing Computed Tomography Image Quality and Radiation Protection in Radiology: Systematic Review and Meta-Analysis. *Journal of Medical Internet Research*, 27, e66622.
- [16] Rauf, A., et al. (2025). Potential of Artificial Intelligence for Radiation Dose Reduction in Computed Tomography: A Scoping Review. *Radiography*, 31, 102891.
- [17] Abhisheka, B., et al. (2024). Recent Trend in Medical Imaging Modalities and Their Applications in Disease Diagnosis: A Review. *Multimedia Tools and Applications*, 83, 43035–43070.
- [18] Husseiny, D., et al. (2022). How Does Artificial Intelligence in Radiology Improve Efficiency and Health Outcomes? *Pediatric Radiology*, 52, 2087–2093.

